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# Preliminary Study on the Fabrication of Multi-Layer Screen-Printed Electrode for Biosensor Application

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**Abstract.** A biosensor is an analytical device that combines certain biological and physical elements. Several types of transducers are used for physical elements, such as optical, electrochemical, thermic, or gravimetric. Nowadays, electrochemical transducers have become widely used for the application of biomedical sensors. Electrochemical measurement devices called screen-printed electrodes (SPEs) are created by printing several types of ink on a ceramic or plastic substrate. SPEs enable speedy in-situ examination with high repeatability, sensitivity, and accuracy. In this study, SPEs were fabricated using a personalized CNC machine with carbon conductive ink as the electrode and polyethylene terephthalate (PET) as the substrate. The mask, stencil, and screen-printing dimensions were measured using a DinoLite microscope. SPEs characterization was performed using Scanning Electron Microscopy (SEM) to observe the surface morphology. This simple approach method shows a promising result that SPEs can be produced up to 5 screen printing layers with the ability to flow the electrical current under a resistance of  $350.4 \text{ K}\Omega$ .

Keywords: Biosensor; Electrochemical; PET; Screen-printed electrode

# 1. Introduction

The screen-printed electrode is an electrode arrangement commonly used in biomedical sensor applications, consisting of a working electrode, reference electrode, and counter electrode. The screen-printing technique uses a mesh to support the stencil and an emulsion to hold the ink. During the screen-printing process, the squeegee will move across the screen stencil to press a printed material (i.e., ink) through the mesh. In printing multiple layers of ink, it is necessary to ensure that the previously printed ink is first thermally compacted. Finally, it is possible to apply protective ink to isolate the conductive path between the electrodes (Li et al., 2012).

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A procedure to improve the electrode layer is pretreatment on a polyethylene terephthalate (PET) substrate. The main objective of the treatment is to remove the insulating polymer on the polyethylene (Haque et al., 2017), and increase the surface roughness. In addition, this treatment ensures the precision and quality of screen-printing results, where ink adhesion can be greatly affected by the hydrophilicity or hydrophobicity of the substrate. In addition, the hydrophilicity of the suitable substrate is favorable for the adhesion of carbon inks and adds to the excellent electrochemical performance (Du et al., 2016).

SPEs for biosensor applications have been developed with various materials and modifications to detect specific analytes. Table 1 describes in detail various studies related to SPE, which are explicitly used as electrodes for dopamine biosensors, and includes some characteristics of each modification.

Materials	Analytes	Sensitivity	Linear Range	LOD	References
SPCE/rGO/PNR/AuNP	Dopamine	13.38 μA/mM	0.57-500 μM	0.17 μΜ	(Altun et al., 2020)
SPCE/GQD	Dopamine and tyrosine	-	0.1–1000.0 μM dopamine and 1.0–900.0 μM tyrosine	0.05 μM dopamine and 0.5 μM tyrosine	(Beitollahi et al., 2018)
SPCE/GR/p-AHNSA	Dopamine and 5- hydroxytryptamine	-	0.05–100 μM dopamine dan 0.05–150 μM 5– HT	2 nM dopamine and 3nM 5- HT	(Raj et al., 2017)
SPCE/rGO	Uric acid, ascorbic acid, and dopamine	-	10-3000 μM uric acid, 0.1- 2.5 μM, & 5.0-2 × 104 μM ascorbic acid, dan 0.2-80.0 μM & 120.0-500 μM dopamine	0.1 μM uric acid, 50.0 μM ascorbic acid dan 0.4 μM dopamine	(Kanyong et al., 2016)
SPE/ mMWCNTs	Dopamine	-	5-180 μΜ	0.43 µM	(Zhang et al., 2017)
SPCE/CB-ERGO	Dopamine, epinephrine, and paracetamol	16.7 AM <sup>-</sup> <sup>1</sup> Lcm <sup>-2</sup> dopamine, 1.44 AM <sup>-</sup> <sup>1</sup> Lcm <sup>-2</sup> epinephrine, and 0.311 AM <sup>-1</sup> Lcm <sup>-2</sup> paracetamol	$4.9 \times 10^{-6} -$ $1.9 \times 10^{-5} \text{ mol/L}$ dopamine, $9.9 \times 10^{-6} -$ $9.5 \times 10^{-5} \text{ mol/L}$ epinephrine and $9.9 \times 10^{-6} -$ $9.5 \times 10^{-5} \text{ mol/L}$ paracetamol	4.1×10 <sup>-7</sup> M/L dopamine, 1.8×10 <sup>-6</sup> M/L epinephrine , and 1.5×10 <sup>-6</sup> M/L paracetamol	(Ibáñez-Redín et al., 2018)
SPCE/grafit/nafion	Dopamine	2.47 μA μM <sup>-1</sup> cm <sup>-2</sup>	0.5-70 μM	0.023 μM	(Ku et al., 2013)
SPCE/GQD/IL	Ascorbic acid, dopamine, and uric acid	-	25–400 μM ascorbic acid, 0.2–15 μM dopamine, dan 0.5–20 μM uric acid	6.64 μM ascorbic acid, 0.06 μM dopamine, and 0.03 μM uric acid	(Kunpatee et al., 2020)
SPGNE	Ascorbic acid, dopamine, and uric acid	-	40–4500 μM ascorbic acid, 0.5–2000 μM dopamine, dan 0.8–2500 μM uric acid	0.95 μM uric acid, 0.12 μM dopamine, and 0.20 μM uric acid	(Ping et al., 2012)

**Table 1** Recent studies of SPCE in dopamine biosensor applications.

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Materials	Analytes	Sensitivity	Linear Range	LOD	References
SPGE/OPPF	Dopamine	-	1.0 μM-2.5mM	0.5 μΜ	(Ping et al., 2010)
SPCE/CuCrO2-TiO2	Dopamine	16.82 μΑ μΜ <sup>-</sup> 1 cm <sup>-2</sup>	1-230 µM	0.14 μΜ	(Keyan et al., 2021)
SPCE	Dopamine	-	-	0.09 μmol L- 1	(Cagnani et al., 2020)
SPE/HP-AuNPs	Dopamine	-	10 <sup>-7</sup> –10 <sup>-3</sup> M	3 × 10 <sup>-8</sup> M	(Varodi et al., 2020)
SPE/rGO-CDBA-Lac	Dopamine	-	0.1–70 μM,	0.03 µM	(Hua et al., 2015)
SPC/AuNPs	Dopamine dan 5- HIAA	-	0.2–100 μM dopamine and 0.5–200 μM 5- HIAA	8 nM dopamine and 22 nM 5-HIAA	(Gupta et al., 2015)
SPCE/MWCNT-GNP dan SPCE/GPH-GNP	Dopamine	$\begin{array}{c} 252.5\pm6.44\\ \mu A \ L \ cm^{-2}\\ mmol^{-1} \ using\\ SPCE/CNT-\\ GNP, \ and\\ 474.2\pm11.09\\ \mu A \ L \ cm^{-2}\\ mmol^{-1} \ using\\ SPCE/GPH-\\ GNP \end{array}$	0.2–400 µmol L <sup>-1</sup> using SPCE/MWCNT- GNP, and 0.03– 150 µmol L <sup>-1</sup> using SPCE/GPH-GNP	60 nmol L <sup>-1</sup> using MWCNT- GNP/C SPE, and 10 nmol L <sup>-1</sup> using graphene- GNP/C SPE	(Stoytcheva et al., 2016)
SPCE/ZnO/rGO/AuNP	Dopamine	-	0.5–100 μM	0.294 µM	(Gu et al., 2022)
SPE-TiO2	Dopamine	462 nA mM <sup>-1</sup> cm <sup>-2</sup>	200-1500 μM	20 µM	(Tavella et al., 2018)
SPCE/2D-MoS <sub>2</sub> nanosheet	Dopamine and tyrosine	$1044 \ \mu A \ mM^{-1} \ cm^{-2} \ dopamine \ and \ 321 \ \mu A \ mM^{-1} \ cm^{-2} \ tyrosine \ dot \ d$	1–100 μM dopamine and 1–500 μM tyrosine	0.085 μM dopamine and 0.5 μM tyrosine	(Zribi et al., 2020)
SPCE/AuNP	Dopamine and riboflavin	550.4 μA mM <sup>-1</sup> cm <sup>-2</sup> dopamine dan 2399 μA mM <sup>-1</sup> cm <sup>-2</sup> riboflavin	2–100 μM dopamine and 2–70 μM riboflavin	0.22 μM dopamine and 0.067 μM riboflavin	(Chelly et al., 2021)
SPCE-FR4 substrate	-	-	-	-	(Charmet et al., 2020)
SPCE/PPy/TA/CTAB	Dopamine	0.039 μΑ μΜ <sup>-</sup> 1	0.5-100 μM	2.9 × 10 -7 M	(Abdi et al., 2021)

Some of the summaries above show how powerful SPCE performance is when applied to the dopamine biosensor. In addition, research conducted by Charmet et al. also shows that the homemade method of fabrication with a simple approach can also produce sensors with competitive performance (Charmet et al., 2020). In the formation of SPCE, research conducted by Randviir et al. used a screen-printing method with silver/silver chloride as a reference electrode (Randviir et al., 2014). The next layer is carbon ink printed on a counter layer and working electrode, as well as a liaison between the three electrodes printed on a flexible polyester (PE) substrate. Subsequently, the dielectric paste will be printed on the substrate and dried at 60°C for 30 minutes before the SPCE is ready for use. This study aimed to fabricate screen printing electrodes using a personalized CNC machine for screen printing purposes using conductive carbon as electrode ink and polyethylene terephthalate (PET) as substrate.

### 2. Methods

Conductive carbon ink was purchased from mjstation (Tangerang). Polyethylene terephthalate (PET) was purchased from the Emake store (China). Screen emulsion liquid (photoxol 188), screen printing sensitizer, superxol m-3 diluent, superxol 3 stencil remover, T180 mesh screen, and screen-printing squeegee were purchased from Provenio Indonesia. The voltammetric characterization used EmStat4s LR with the PSTrace 5.9 interface (PalmSens, Netherlands). A personalized CNC 3018 Pro tabletop machine for screen printing and an HP LaserJet Pro MFP M117fw printer for making masks were obtained from the Manufacturing Research Center (MRC FTUI).

### 2.1. Electrochemical Cell Design

Figure 1 is an electrochemical cell design using the Inventor 3D design application. The electrochemical cell's geometry follows a typical electrochemical cell geometry (de Araujo & Paixão, 2014), with modifications to the electrode legs to match the PalmSens SPE adapter.



Figure 1 Electrochemical cell geometry design

### 2.2. Screen-Printing Mask Fabrication

The electrochemical cell design will be printed on Yashica transparent paper. The process uses an HP LaserJet Pro MFP M117fw printer. The result of the electrochemical cell design on Yashica transparent paper is called a mask. The mask is then used to make stencils for screen printing using photolithography.

### 2.3. Screen-Printing Stencil Fabrication

Screen printing is coated with screen emulsion liquid (Superxol 188) mixed with a sensitizer in a successive ratio of 5:1, then mixed and poured over the screen evenly. Furthermore, it will be dried at low light intensity at room temperature for 25 minutes, followed by the transfer of the design from the mask to the screen printing by a photolithography method using a 40-watt lamp for 14 minutes. In the following process, the development process will be carried out by flushing the formed SPE with pressurized water to identify the screen's resistance.

### 2.4. Screen-Printing Process

Figure 2 shows a screen-printing scheme with carbon as the ink paste for the process. The substrate used is polyethylene terephthalate (PET). The printing process takes place using a personalized CNC 3018 Pro machine. It occurs when the squeegee presses the screen to initiate contact between the screen and the substrate, and the ink will be pushed down into the opening, a permeable area that forms the desired image.

Parameters in the screen-printing process are the mesh screen size, the snap offdistance, and the number of layers of screen printing. The mesh screen size used is T180, where the code T (tick) is a term commonly used in Asia to denote the number of threads sewn every 1 cm. The higher T value results in tighter stitches and more precise screen printing. Snap-off distance is the distance between the substrate and the screen printing; while the snap-off distance applied in this study is 2.5mm, and the screen-printing process layer consists of 5 layers. Each layer of the ink screen printing process is dried for 15 minutes at room temperature, followed by 30 minutes of drying at a temperature of 70° C after the desired number of layers has been achieved. The overall process of fabricating the screen printing electrode is shown in Figure 2.



Figure 2 Fabrication of screen printing electrode

# 3. Results and Discussion

# 3.1. Screen-printing Stencil

The irradiation time was varied in the stencil fabrication process on the T180 screen. There is a difference in the results of the stencil formation at each time variation. The irradiation time that formed the best stencil was 14 minutes. Within 8 to 12 minutes, the emulsion on the screen was damaged and did not form the desired SPE stencil when the development process was applied with pressurized water. Meanwhile, at 16 to 18 minutes, the emulsion on the screen is challenging to develop due to prolonged irradiation time. The optimum duration for irradiation is 14 minutes. Figure 3 shows the photolithographic process using a 40-watt light source. The light source consists of five T5 LED lamps arranged in parallel. Lighting level affects irradiation time to get appropriate stencil. The higher lighting level requires less irradiation time. However, if the irradiation time is too long, the development process cannot occur.



# Figure 3 Photolithography process

# 3.2. Microscope

The mask observation for screen-printing was measured using a DinoLite microscope. It is done on the straight-line section of the SPE. Figure 4 shows the results of mask measurements for screen printing.



# Figure 4 Screen printing mask dimension

The print quality using the HP LaserJet Pro MFP M117fw printer is relatively acceptable. The mask works well since it can withstand the light from the photolithography process to produce a stencil on the screen.



Figure 5 Dimensional comparison graph of the initial design and the printed mask.

In this process, there are dimensional differences between the initial design and the printed mask. Figure 5 shows the print capability of the HP LaserJet Pro MFP M117fw printer on YASHICA paper. The most significant deviation between the design and print dimensions is 0.485 mm, and the slightest deviation is 0.469 mm. So, it can be concluded that the HP LaserJet Pro MFP M11fw printer machine can print an average dimension of approximately 0.977 $\pm$ 0.008 mm (977 µm).

The screen printing stencils used in fabricating 5-layer SPE required a set with a mesh size of T180 and a snap-off distance of 2.5 mm. The following stencil results from photolithography using a mask, as described previously. Figure 6 shows changes in the dimensions of the stencil when it is used for the screen-printing process ten times.



Figure 6 Dimensional comparison of (a) the initial stencil and (b) the stencil after ten times use

It is seen that the initial stencil dimensions are similar to the mask size. The change in dimension is because the stencil edges are not perfectly exposed to the light source due to the diffused light source during the photolithography process. It causes the particular area to not be scattered apart during the development process. Figure 6b shows that the Dimensional changes after the screen printing process that can be caused by multiple cleaning of the screen from ink. In the screen printing process, the screen needs to be cleaned with superxol M-3 liquid each time. When used repeatedly, the liquid possibly removes or damages the hardened emulsion liquid on the screen. When the layers increase, the dimensions tend to be larger than the previous layer.

Figure 7 depicts the difference between the initial stencil's average width and the stencil's width after ten times use.



Figure 7 Dimension comparison graph of initial and ten times use a stencil

The average dimensions of the initial stencil T180 are approximately  $0.742\pm0.031$  mm (742 µm), and the dimensions of the stencil after ten uses are approximately  $1.084\pm0.127$  mm. The dimensional deviation between the mask and the initial stencil was 13.64%, while the stencil after ten uses was 18.69%.

The screen-printing process involves polyethylene terephthalate (PET) substrates with different coating levels.



**Figure 8** SPE screen printing of the (a) first and (b) second layers

The results of the observations between the first and second layers of the prepared SPEs are shown in Figures 8a and 8b. The PET substrate has a hydrophobic character and low compound absorption, which causes the insufficient formation of the carbon ink base (Zhang et al., 2021). In order to further improve the hydrophilicity of PET substrate, O<sub>2</sub> plasma technique can be performed (Du et al., 2016).



Figure 9 SPE screen printing of the (a) third and (b) fourth layers

However, it gradually improves as the number of layers increases. Results of SPE observations third layer (Figure 9a) has a better structure than the first and second layers since its carbon ink already has a stronger base than the previous layers. Figure 9b shows that the side part of the fourth layer is unacceptable due to changes in the stencil's shape from repeated cleaning with superxol M-3 liquid. The carbon ink density of the two layers above is more promising than the previous ones, but it is still unsatisfactory to detect the current.

When the fifth layer was fabricated, the density of the electrodes increased, but there was a visually significant change in size. Figure 10 shows an unsatisfactory result compared to the expected design on the surface of the fifth layer, particularly on the side of the electrode path. As described earlier, it is caused by a change in the stencil's shape.



### Figure 10 SPE screen printing fifth layers

When the fifth layer was fabricated, the density of the electrodes increased, but there was a visually significant change in size. Figure 10 shows an unsatisfactory result compared to the expected design on the surface of the fifth layer, particularly on the side of the electrode path. As described earlier, it is caused by a change in the stencil's shape.

From this phenomenon, the average width of the dimensions for each additional layer can be observed. Figure 11 shows that the higher the layer on the PET substrate, the larger the dimensions. Significant dimensional changes can be seen once the SPE reaches the fourth layer. These dimensional changes can occur due to the repeated use of superxol m-3 liquid. The average dimension in the first layer is  $0.977\pm0.148$  mm;  $1.022\pm0.145$  mm in the second layer,  $1.105\pm0.074$  mm in the third layer,  $1,298\pm0.146$  mm in the fourth layer; and  $1.536 \pm 0.184$  mm in the fifth layer.

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## 3.3. Scanning Electron Microscope (SEM)

Cross-sectional testing using SEM was conducted to determine the change in thickness dimensions of the screen printing on the first and fifth layers. Figure 12a shows that the consistency of carbon ink on the PET substrate is not satisfactory at the first layer. It shows that the limitation in the SPE manufacturing base layer will prevent the current from passing through the SPE. Figure 12b shows that the carbon ink density at the fifth layer looks more acceptable but still develops varying heights.





Figure 13 shows that the fifth layer has a reasonably significant thickness deviation influenced by the arrangement of the previous layers. The most substantial effect is due to the first layer, an SPE base with poor density, which causes a significant difference in the height of the following layers. Therefore, the fifth layer has a considerable deviation in thickness.



Figure 13 Thickness dimension comparison graph of SPE first and fifth layers

In addition, the SEM was carried out from the cross-sectional view, while research conducted by Randviir et al. performed SEM testing from the top view and tested several SPE models, namely edge plane-like SPE (ESPE), basal plane-like SPE (BSPE), and graphene SPE (GSPE) (Randviir et al., 2014). ESPE and GSPE have relatively rough and irregular surface characteristics, while BSPE has a smoother surface than ESPE and GSPE.

# 4. Conclusions

Based on the work that has been demonstrated, it can be concluded that the SPE fabrication process using carbon ink on a PET substrate can be up to 5 layers but still has not achieved the geometric results according to the initial design. The fabrication process in the first and second layers has a low ink density, and the current has been unable to pass through the electrode path due to the hydrophobic nature of the substrate. In the third layer, SPE has a better characteristic than the previous layer because it has more robust surface roughness than the previous layer, resulting in a better bond of carbon ink on the third layer. In the fourth and fifth layers, the stencil has been deformed due to the multiple screen cleanings, which increased the electrode width. In the fifth layer, the current can be generated with a resistance of 350.4 K $\Omega$ . The morphological characterization of SPEs presented using SEM shows that the fifth layer has a significant thickness deviation influenced by the arrangement of the previous layers. This work can be used as an initial step to conduct further research on SPEs fabrication, which can later be beneficial in various applications.

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### References

- Abdi, M.M., Azli, N.F.WM., Chaibakhsh, N., Lim, H.N., Tahir, P.M., Karimi, G.,Khorram, M., 2021. Nonenzymatic Dopamine Biosensor Based on Tannin Nanocomposite. *Journal of Polymer Science*, Volume 59(5), pp. 428–438
- Altun, M., Bilgi Kamaç, M., Bilgi, A., Yilmaz, M., 2020. Dopamine Biosensor Based on Screen-Printed Electrode Modified with Reduced Graphene Oxide, Polyneutral Red and Gold Nanoparticle. *International Journal of Environmental Analytical Chemistry*, Volume 100(4), pp. 451–467
- Beitollahi, H., Dourandish, Z., Ganjali, M.R., Shakeri, S., 2018. Voltammetric Determination of Dopamine in the Presence of Tyrosine Using Graphite Screen-Printed Electrode Modified with Graphene Quantum Dots. *Ionics*, Volume 24(12), pp. 4023–4031
- Cagnani, G.R., Ibáñez-Redín, G., Tirich, B., Gonçalves, D., Balogh, D.T., Oliveira, O.N., 2020. Fully-printed Electrochemical Sensors Made with Flexible Screen-Printed Electrodes Modified By Roll-To-Roll Slot-Die Coating. *Biosensors and Bioelectronics*, Volume 165, p. 112428
- Charmet, J., Rodrigues, R., Yildirim, E., Challa, P.K., Roberts, B., Dallmann, R., Whulanza, Y., 2020. Low-Cost Microfabrication Tool Box. *Micromachines*, Volume 11(2), p. 135
- Chelly, S., Chelly, M., Zribi, R., Gdoura, R., Bouaziz-Ketata, H., Neri, G., 2021. Electrochemical Detection of Dopamine and Riboflavine on a Screen-Printed Carbon Electrode Modified by AuNPs Derived from Rhanterium suaveolens Plant Extract. *ACS Omega*, Volume 6(37), pp. 23666–23675

- de Araujo, W.R., & Paixão, T.R.L.C., 2014. Fabrication of Disposable Electrochemical Devices Using Silver Ink and Office Paper. *The Analyst*, Volume 139(11), pp. 2742–2747
- Du, C.X., Han, L., Dong, S.L., Li, LH., Wei, Y., 2016. A Novel Procedure for Fabricating Flexible Screen-Printed Electrodes with Improved Electrochemical Performance. *IOP Conference Series: Materials Science and Engineering*, Volume 137, p. 012060
- Gu, M., Xiao, H., Wei, S., Chen, Z., Cao, L., 2022. A Portable and Sensitive Dopamine Sensor Based on Aunps Functionalized ZnO-rGO Nanocomposites Modified Screen-Printed Electrode. *Journal of Electroanalytical Chemistry*, Volume 908, p. 116117
- Gupta, P., Goyal, R.N., Shim, Y.-B., 2015. Simultaneous Analysis of Dopamine and 5-Hydroxyindoleacetic Acid at Nanogold Modified Screen Printed Carbon Electrodes. *Sensors and Actuators B: Chemical*, Volume 213, pp. 72–81
- Haque, S.M., Rey, J.A.A., Masúd, A.A., Umar, Y., Albarracin, R., 2017. Electrical Properties of Different Polymeric Materials and their Applications: The Influence of Electric Field. *In* B. Du (Ed.), Properties and Applications of Polymer Dielectrics. InTech
- Hua, Z., Qin, Q., Bai, X., Wang, C., Huang, X., 2015. β-Cyclodextrin Inclusion Complex as the Immobilization Matrix for Laccase in the Fabrication of a Biosensor for Dopamine Determination. *Sensors and Actuators B: Chemical*, Volume 220, pp. 1169–1177
- Ibáñez-Redín, G., Wilson, D., Gonçalves, D., Oliveira, O.N., 2018. Low-Cost Screen-Printed Electrodes Based on Electrochemically Reduced Graphene Oxide-Carbon Black Nanocomposites for Dopamine, Epinephrine and Paracetamol Detection. *Journal of Colloid and Interface Science*, Volume 515, pp. 101–108
- Kanyong, P., Rawlinson, S., Davis, J., 2016. A Voltammetric Sensor Based on Chemically Reduced Graphene Oxide-Modified Screen-Printed Carbon Electrode for the Simultaneous Analysis of Uric Acid, Ascorbic Acid and Dopamine. *Chemosensors*, Volume 4(4), p. 25
- Keyan, A.K., Yu, C.-L., Rajakumaran, R., Sakthinathan, S., Wu, C.-F., Vinothini, S., Ming Chen, S., Chiu, T.-W., 2021. Highly Sensitive and Selective Electrochemical Detection of Dopamine based on CuCrO<sub>2</sub>-TiO<sub>2</sub> Composite Decorated Screen-Printed Modified Electrode. *Microchemical Journal*, Volume 160, pp. 105694
- Ku, S., Palanisamy, S., Chen, S.-M., 2013. Highly Selective Dopamine Electrochemical Sensor Based on Electrochemically Pretreated Graphite and Nafion Composite Modified Screen Printed Carbon Electrode. *Journal of Colloid and Interface Science*, Volume 411, pp. 182–186
- Kunpatee, K., Traipop, S., Chailapakul, O., Chuanuwatanakul, S., 2020. Simultaneous Determination of Ascorbic Acid, Dopamine, and Uric Acid Using Graphene Quantum Dots/Ionic Liquid Modified Screen-Printed Carbon Electrode. Sensors and Actuators B: Chemical, Volume 314, p. 128059
- Li, M., Li, Y.-T., Li, D.-W., Long, Y.-T., 2012. Recent Developments and Applications of Screen-Printed Electrodes in Environmental Assays—A Review. *Analytica Chimica Acta*, Volume 734, pp. 31–44
- Ping, J., Wu, J., Wang, Y., Ying, Y., 2012. Simultaneous Determination of Ascorbic Acid, Dopamine and Uric Acid Using High-Performance Screen-Printed Graphene Electrode. *Biosensors and Bioelectronics*, Volume 34(1), pp. 70–76
- Ping, J., Wu, J., Ying, Y., 2010. Development of an Ionic Liquid Modified Screen-Printed Graphite Electrode and Its Sensing in Determination of Dopamine. *Electrochemistry Communications*, Volume 12(12), pp. 1738–1741
- Raj, M., Gupta, P., Goyal, R.N.,Shim, Y.-B., 2017. Graphene/Conducting Polymer Nano-Composite Loaded Screen Printed Carbon Sensor for Simultaneous Determination of Dopamine and 5-Hydroxytryptamine. *Sensors and Actuators B: Chemical*, Volume 239,

pp. 993–1002

- Randviir, E.P., Brownson, D.AC., Metters, J.P., Kadara, R.O., Banks, C.E., 2014. The Fabrication, Characterisation and Electrochemical Investigation of Screen-Printed Graphene Electrodes. *Physical Chemistry Chemical Physics*, Volume 16(10), pp. 4598–4611
- Stoytcheva, M., Zlatev, R., Gonzalez Navarro, F.F., Velkova, Z., Gochev, V., Montero, G., Ayala Bautista, A.G., Toscano-Palomar, L., 2016. PVA-AWP/Tyrosinase Functionalized Screen-Printed Electrodes for Dopamine Determination. *Analytical Methods*, Volume 8(26), pp. 5197–5203
- Tavella, F., Ampelli, C., Leonardi, S., Neri, G., 2018. Photo-Electrochemical Sensing of Dopamine by a Novel Porous TiO2 Array-Modified Screen-Printed Ti Electrode. *Sensors*, Volume 18(10), p. 3566
- Varodi, C., Pogacean, F., Gheorghe, M., Mirel, V., Coros, M., Barbu-Tudoran, L., Stefan-van Staden, R.-I., Pruneanu, S., 2020. Stone Paper as a New Substrate to Fabricate Flexible Screen-Printed Electrodes for the Electrochemical Detection of Dopamine. *Sensors*, Volume 20(12), p. 3609
- Zhang, Y., Ying, L., Wang, Z., Wang, Y., Xu, Q., Li, C., 2021. Unexpected Hydrophobic to Hydrophilic Transition of PET Fabric Treated in a Deep Eutectic Solvent of Choline Chloride and Oxalic Acid. *Polymer*, Volume 234, p. 124246
- Zhang, Y.-M., Xu, P.-L., Zeng, Q., Liu, Y.-M., Liao, X., Hou, M.-F., 2017. Magnetism-Assisted Modification of Screen Printed Electrode with Magnetic Multi-Walled Carbon Nanotubes for Electrochemical Determination of Dopamine. *Materials Science and Engineering: C*, Volume 74, pp. 62–69
- Zribi, R., Maalej, R., Gillibert, R., Donato, M.G., Gucciardi, P.G., Leonardi, S.G., Neri, G., 2020. Simultaneous And Selective Determination of Dopamine and Tyrosine in the Presence of Uric Acid With 2D-Mos2 Nanosheets Modified Screen-Printed Carbon Electrodes. *FlatChem*, Volume 24, p. 100187